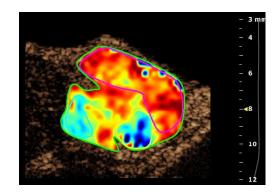
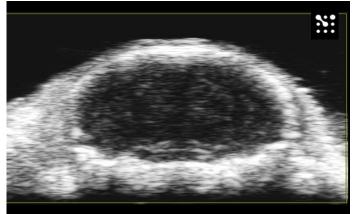


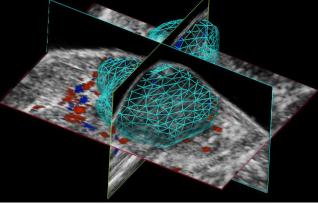


Mouse model and High-frequency ultrasound and Photoacoustic imaging in preclinical research



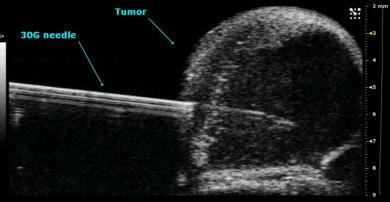






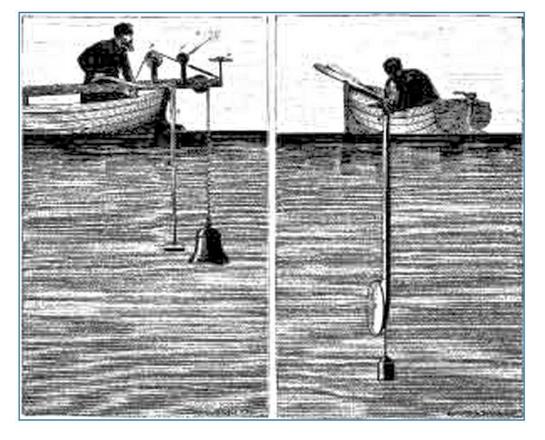
Tiziano Lottini





History of Ultrasounds

In 1826 on Lake Geneva, Switzerland, Jean-Daniel Colladon and Charles-Francois Sturm made the first recorded attempt to determine the speed of sound in water.

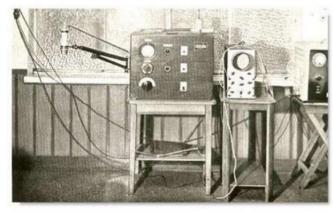


First applications of ultrasounds



The sonar was invented by the American Lewis Nixon in 1906 and was intended to ships to find the **iceberg** in time to avoid collisions. Later, during the First World War, it was developed a special type of sonar suited to detect **submarines**.

History of Ultrasounds



Denier's Ultrasonoscopic apparatus with ultrasound generator, emitter transducer and oscilloscope. This can be adapted for both therapeutic and diagnostic purposes



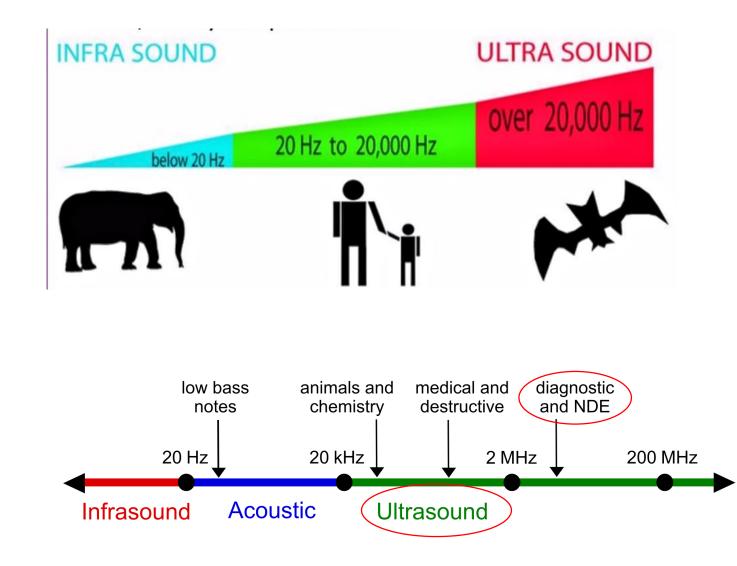
The first hand-held imaging instrument was developed by John Wild and John Reid in the early 1950's

The use of ultrasounds in medicine for diagnostic purposes dates back to 1949 with the first scan by Karl Dussik.

Nowadays ultrasounds are widely used for medical diagnosis

What are Ultrasounds ?

Ultrasound is sound wave with frequencies higher than the upper audible limit of human hearing.

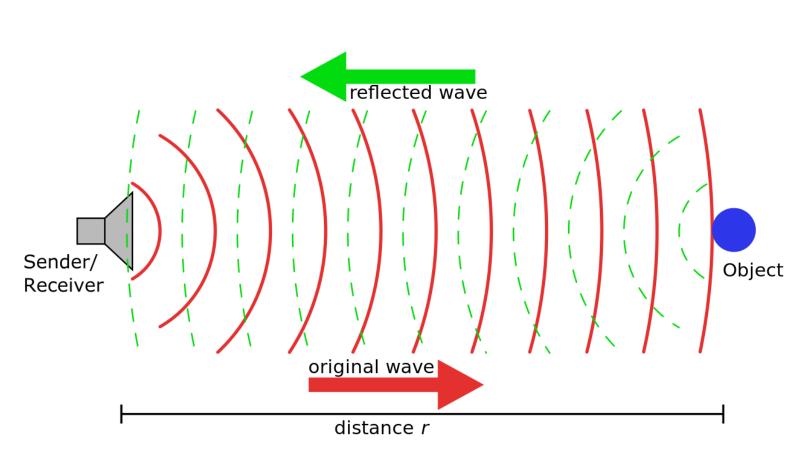


Interaction of Ultrasound with matter:

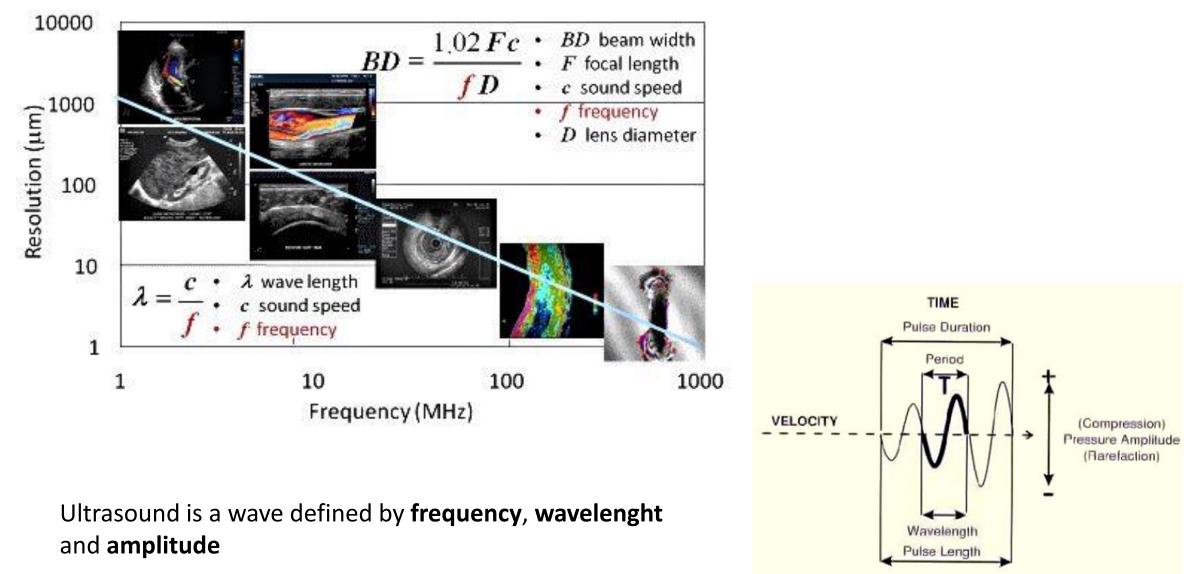
- Reflection
- Transmission
- Attenuation
- Scattering



Deformation of certain materials that result from the application of electric field

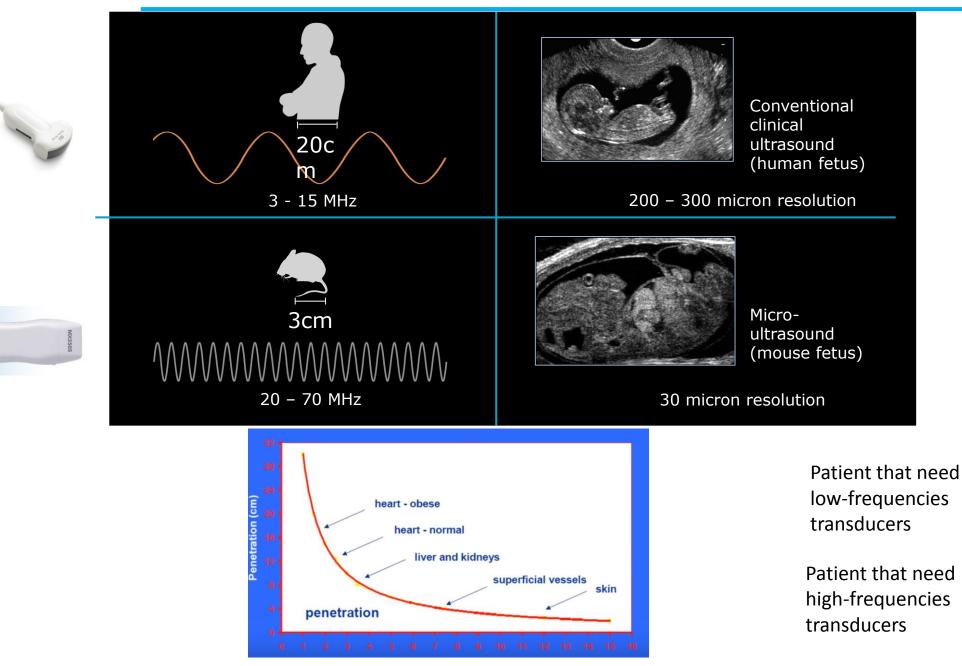


Ultrasound/Micro-Ultrasound

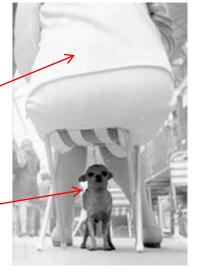


DISTANCE

Micro-Ultrasound

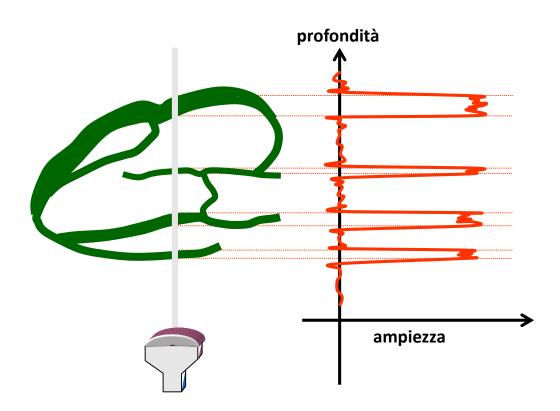


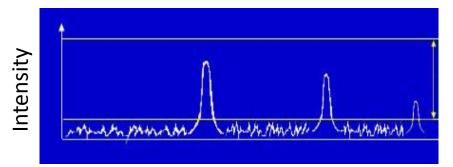
:?



Ultrasound Modes

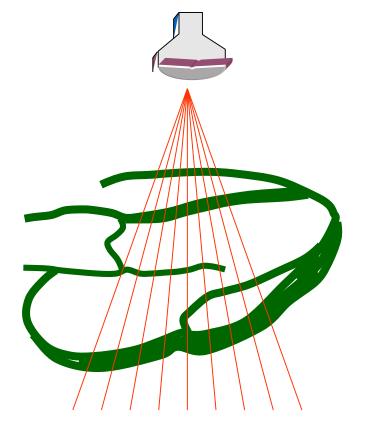
• **A-Mode** (Amplitude Mode). First developed, is the display of amplitude spikes of different heights. A-Mode consists of a x and y axis, where x represents the depth of the echo and y represents the Amplitude. Used in ophtalmology





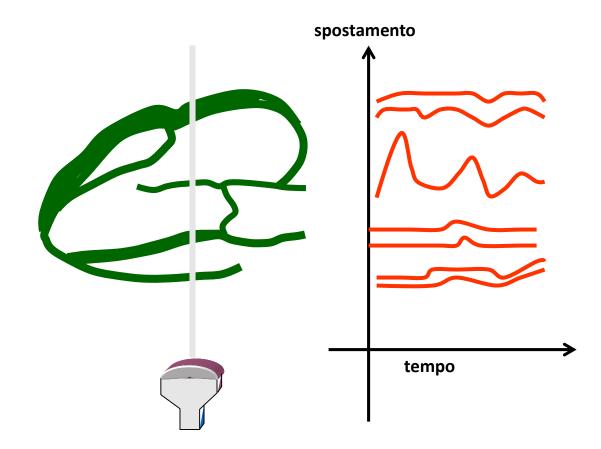
Time (depth of the echo)

•**B-Mode** (Brightness Mode) a linear array of transducers simultaneously scans a plane through the body that can be viewed as a two-dimensional image on screen. The brightness depends upon the amplitude or intensity of the echo. Commonly known as 2D mode.





•**M-Mode** (Motion Mode) is the display of a onedimensional image that is used for analyzing moving body parts commonly in cardiac and fetal cardiac imaging (e.g. cardiac valves).





Ultrasound with VevoLAZR-X

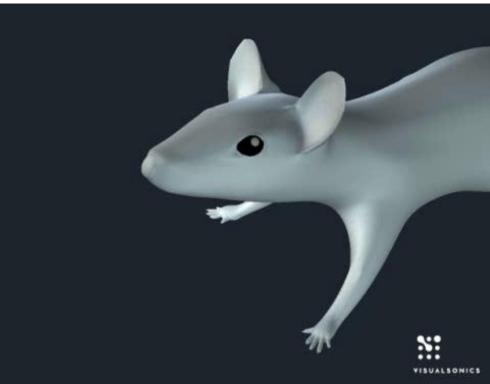




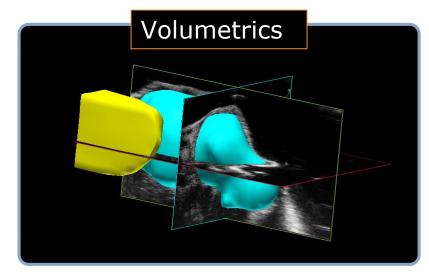
Multimodal imaging sistem

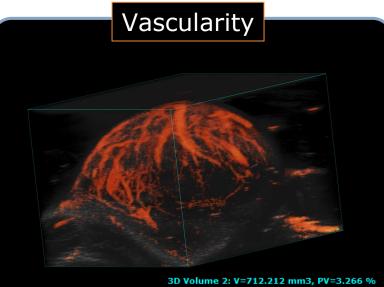
Vevo-LAZR-X

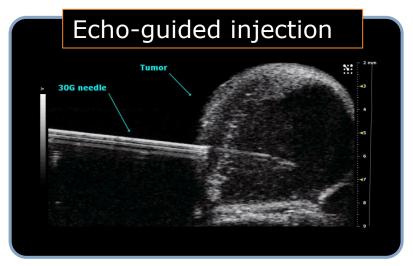
(Visualsonics Fujifilm)

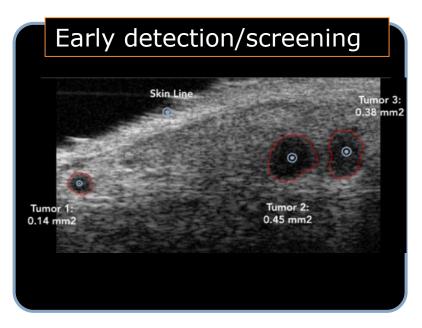


Visualization with micro-ultrasound







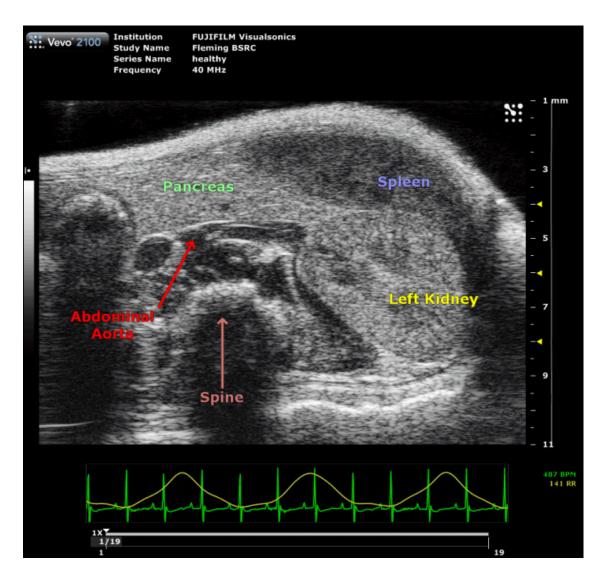


Mouse abdominal echografy

An-echogenic tissue: absence of reflection

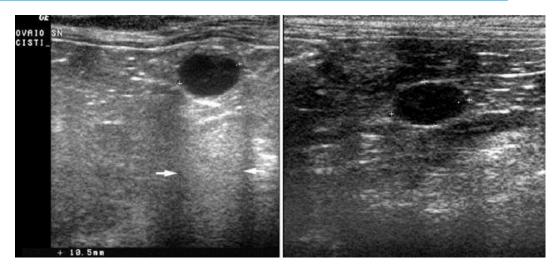
Hyperechogenic tissue: High acoustic impedance (the wave is reflected but not trasmissed)

Hypoechogenic tissue



Artefacts...

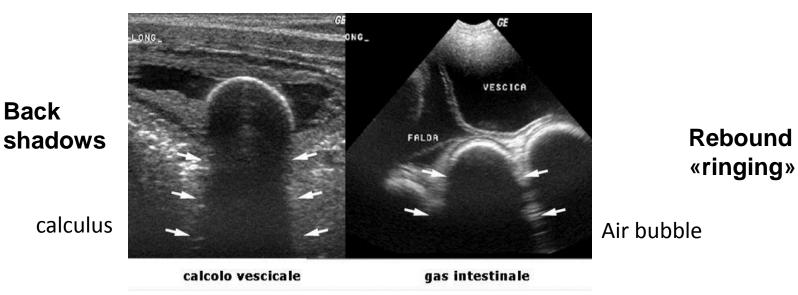
Images or part of images that do not rapresent the real anatomy of the tissue

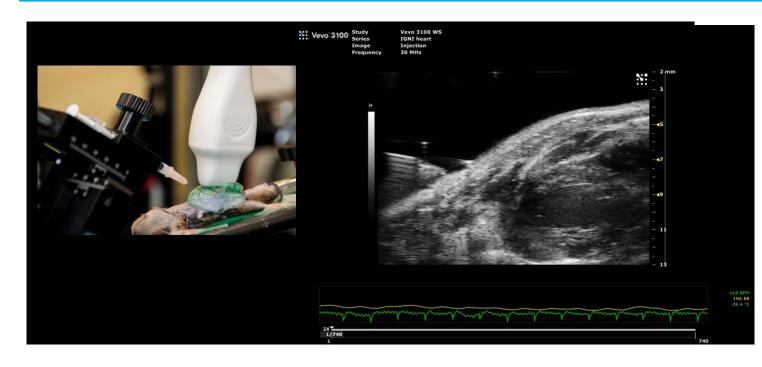


FEGATO DX LONG DORS

Ovarian cysts: Liquid inside, **Back enhancement**, lateral shadow

Lymphomatous lymph node: No Back enhancement

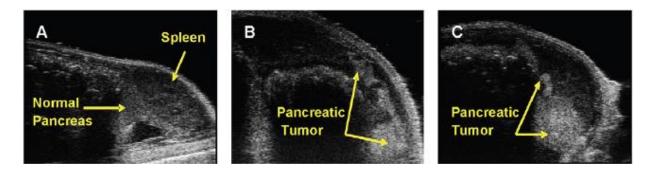


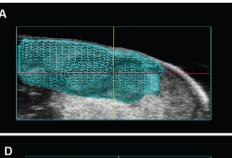


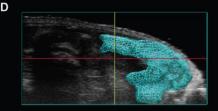
Echo-guided intervention into the heart

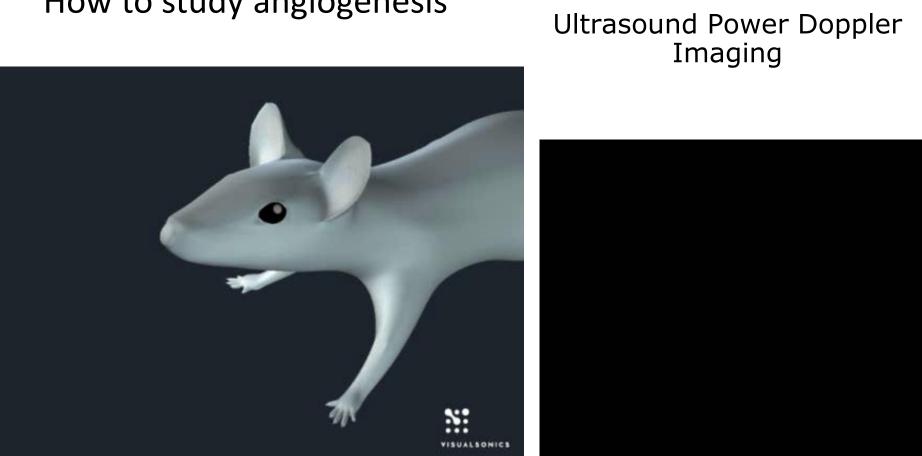
3D volume reconstruction

Monitoring tumor development



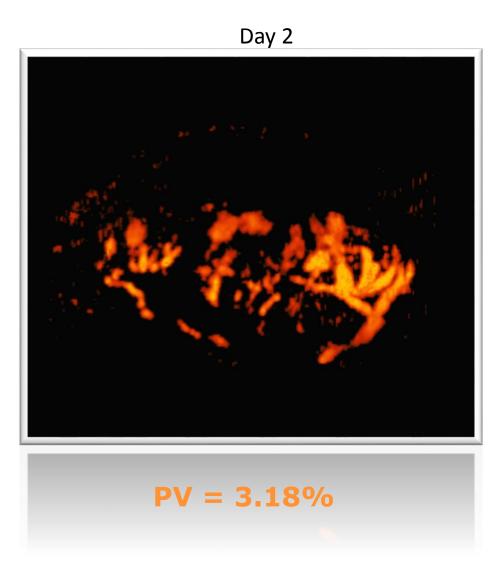


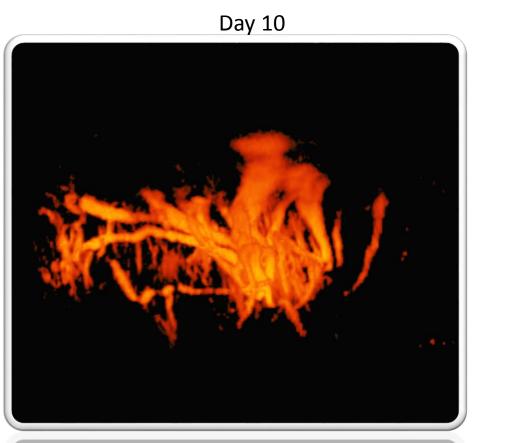




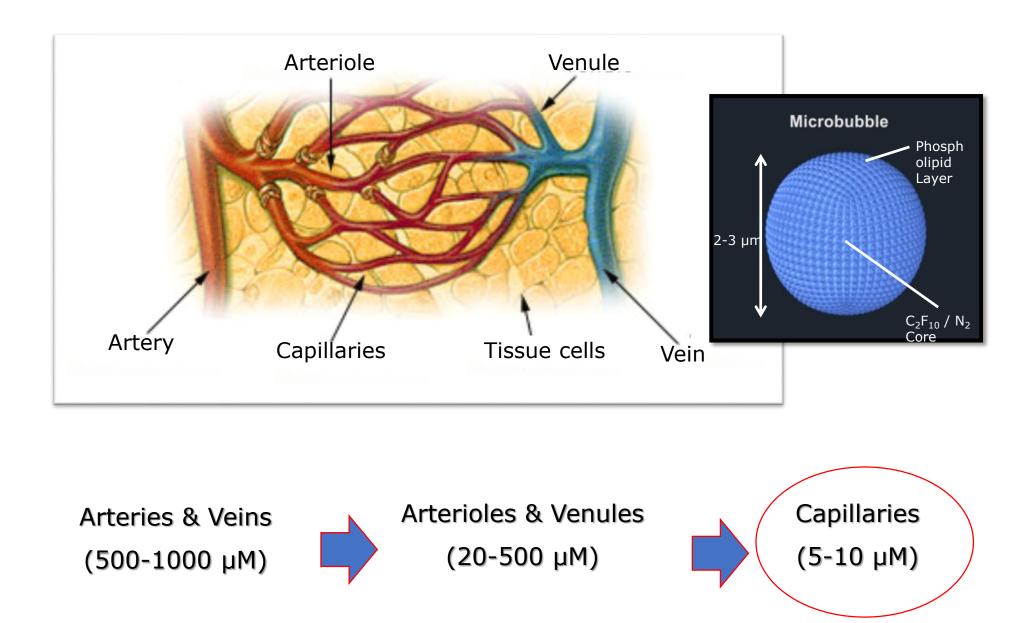
How to study angiogenesis

Power Doppler Mode Imaging

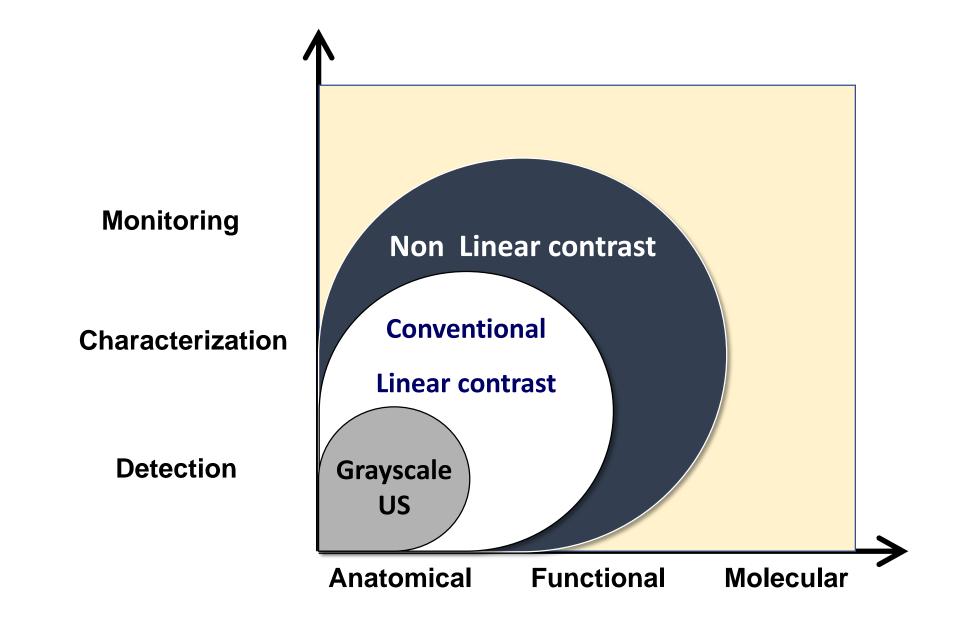




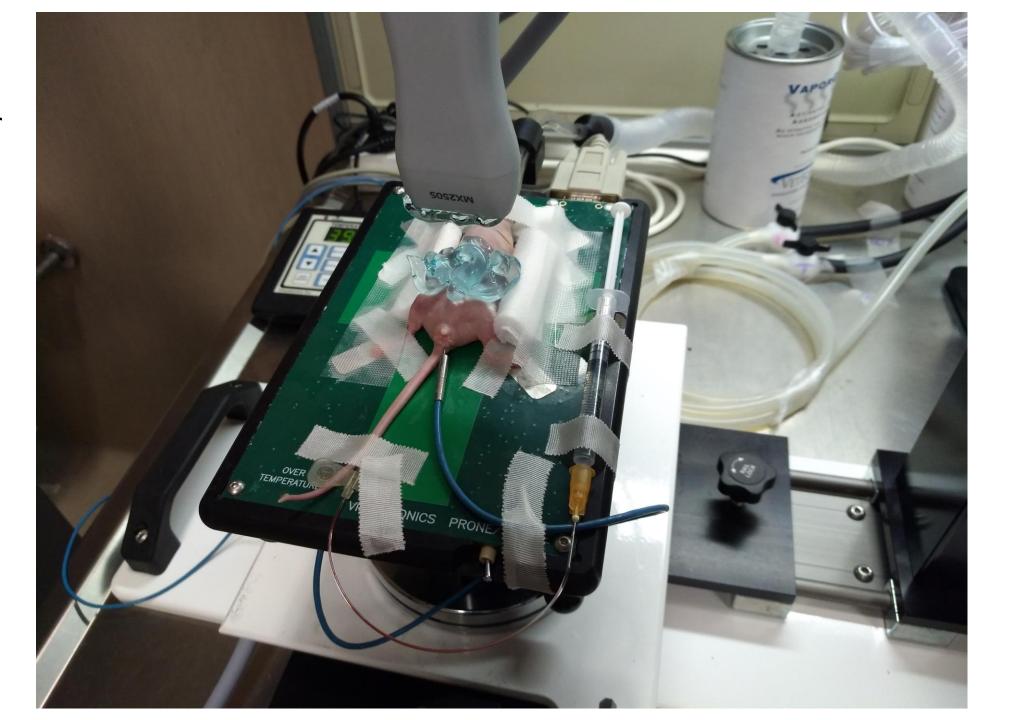
PV = 11.22%



Non Linear contrast imaging

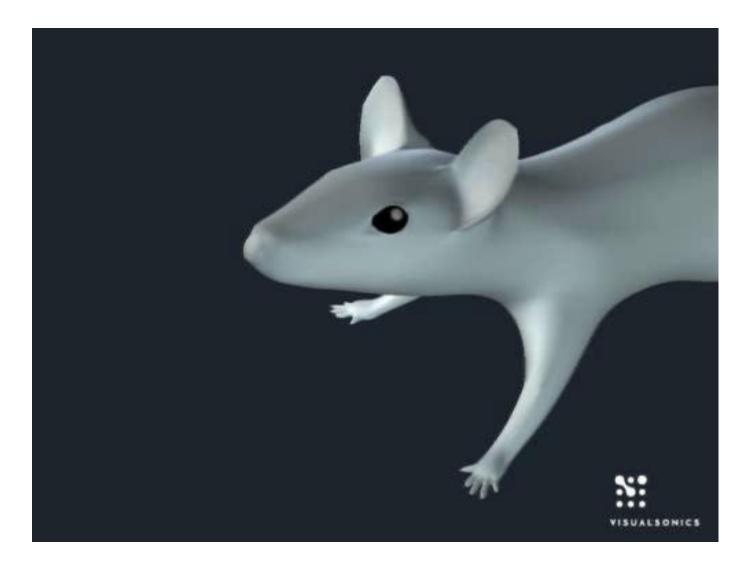


Non-Linear Contrast Mode



Non-Linear contrast imaging

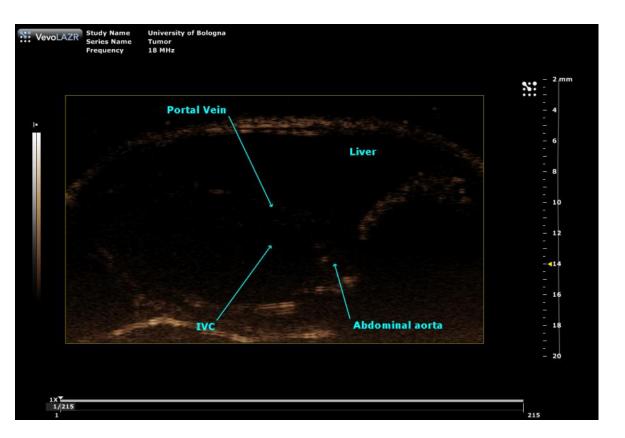
Microbubble applications



Non-Linear contrast imaging

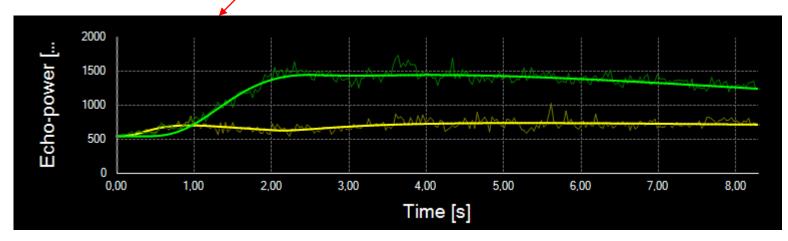
Contrast Enhanced Ultrasound

- The non linear contrast Mode exploit the nonlinear response of the microbubbles to ultrasound pulses
- the goal is to suppress the tissue signal while increasing the detection of the contrast agents, providing a much more sensitive imaging technique

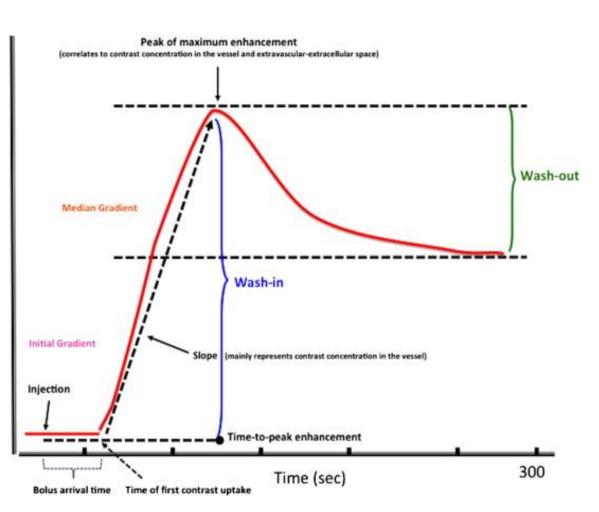


- Contrast-enhanced ultrasound show any selective enhancement in the venous and arterial phases
- Contrast agent uptake may be fast or slow depending on circulation speed





Perfusion curve



Peak Enhancement
Area Under the Curve (Wash-in)
Rise Time
Time To Peak
Wash-in Rate
Wash-in Perfusion Index (WiAUC / RT)

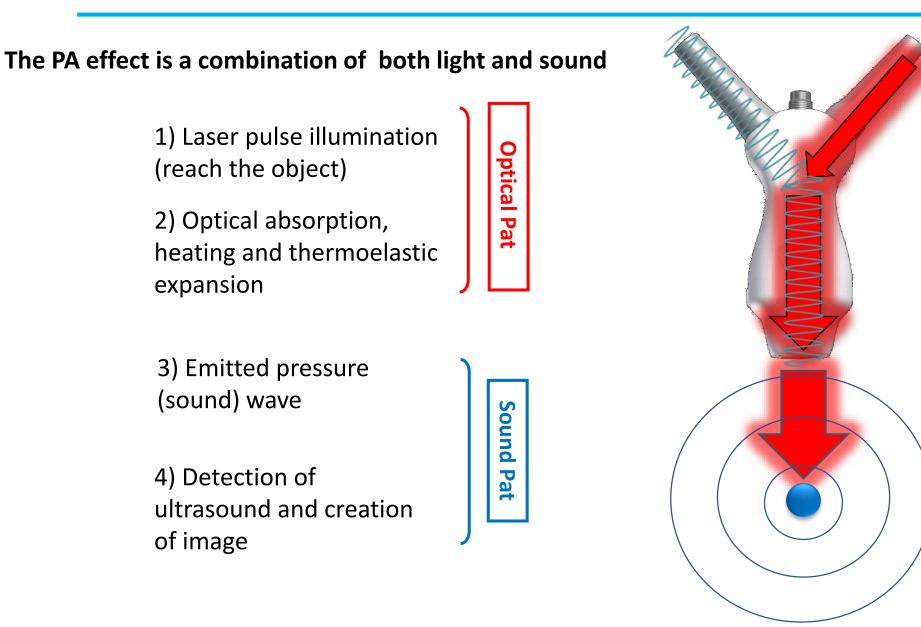
Area	ROI area	
	BASED ON EXTRAPOLATED DATA	

- AUCArea Under the CurvemTTmean Transit Time
- PI Perfusion Index (AUC / mTT)

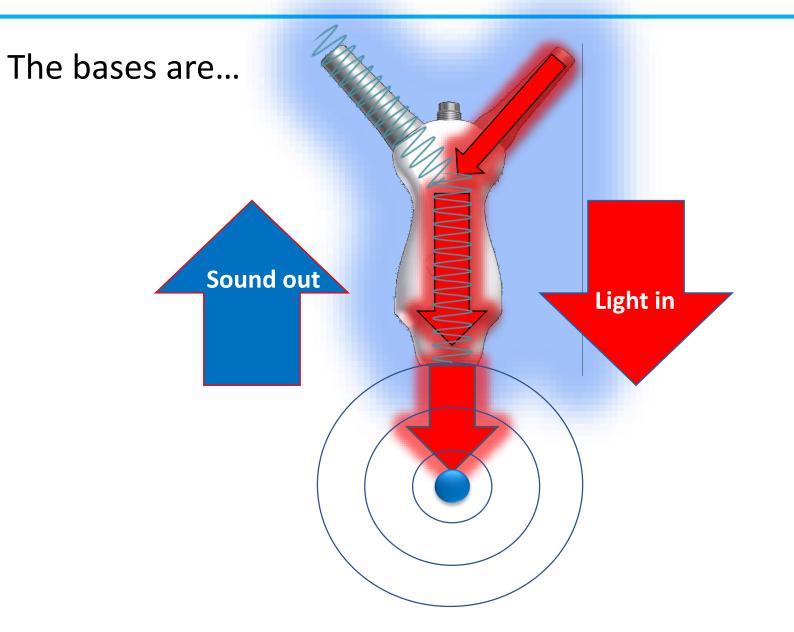
PE = relative blood volume

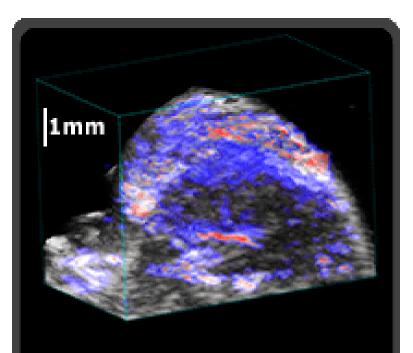
TTP = relative velocity of blood

What is Photoacoustic



What is Photoacoustic





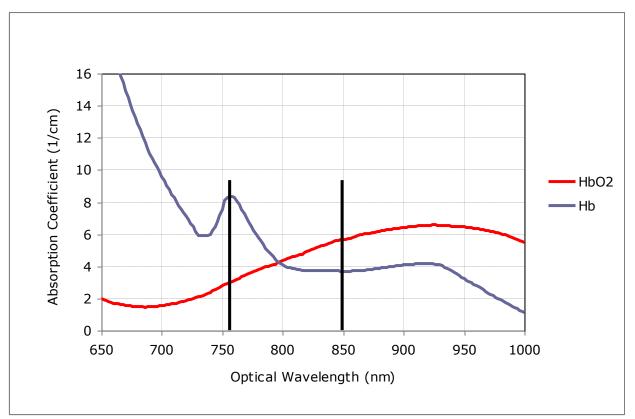
Oxygen saturation in 3D mouse hindlimb tumor Endogenous PA contrast agents

Oxygen Saturation

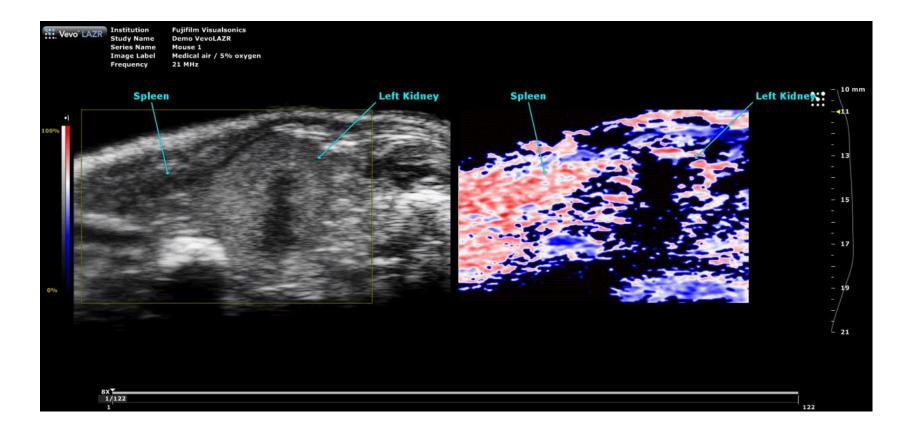
3D Quantification

Oxygen saturation

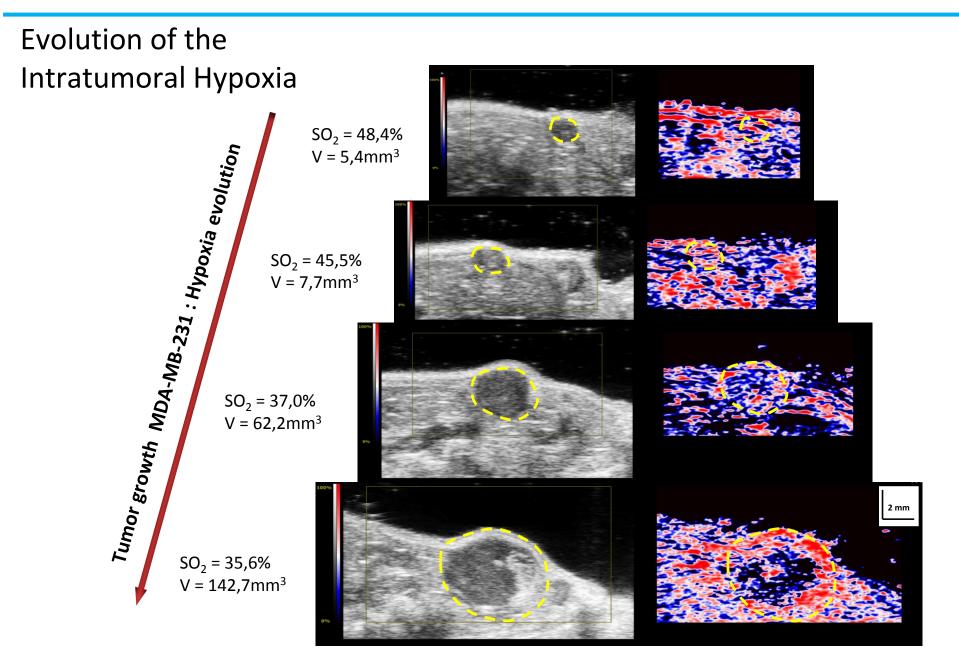




Images are acquired at both **750**nm and **850**nm, an algorithm is applied to create a spectroscopic image of oxygen saturation in real time





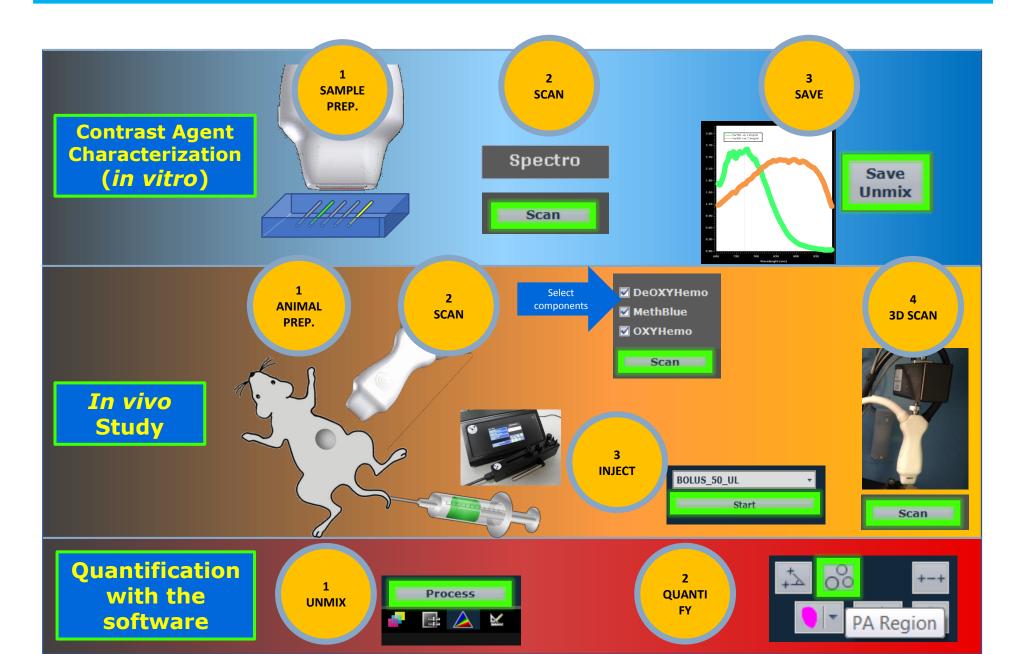


Nanoparticle Tracking with PA analysis

Exogenous PA Contrast Agents

Photoacoustic Contrast Agent	Туре	Absorption Peak (nm)	Size (nm)	Modification Application	Application	Ref.
Indocyanine-green	NIR Fluorescent Dye	810	<2	CarbonNanotube, PEG, PEBBLEs	PAT, in tissue phantoms and <i>in vivo</i>	[7,16–19]
Methylene blue	NIR Fluorescent Dye	650–700	<2		PAT, in tissue phantoms	[15]
Alexa Fluor 750	NIR Fluorescent Dye	750	<2		Multispectral PAI, in vivo	[8,9]
IRDye800CW	NIR Fluorescent Dye	750-800	<2	NPR-1	PAS, in vivo	[13]
IRDye800- c(KRGDf)	NIR Fluorescent Dye	750–790	<2	Integral proteinαvβ3	PAS, in vivo	[20]
Evans Blue	NIR Fluorescent Dye	550	<2		PAT, in vivo	[10]
РРСу-С8	NIR Fluorescent Dye	754–789	<2	Perfluorocarbon	<i>In vivo</i> , dual-modality PAI-FI	[21]
Cypate-C18	NIR Fluorescent Dye	754–790	<2	Perfluorocarbon	<i>In vivo</i> , dual-modality PAI-FI	[21]
Caspase-9 Probe	NIR Fluorescent Dye	640	<2		PAI, in vivo	[11]
MMPSence™ 680	NIR Fluorescent Dye	620, 680	<2		PAI, in tissue phantoms	[14]
BHQ3	Quencher	672	<2		PAI, in vitro	[12]
QXL680	Quencher	680	<2		PAI, in vitro	[12]
Au Nanospheres	Plasmonic Noble Metal Nanoparticle	520-550	20—80	PEG	PAT, in vivo	[22,23]
Au Nanoshells	Plasmonic Noble Metal Nanoparticle	700–1100	50—500	PEG	PAT, in vivo	[24,25]

Molecular Imaging Workflow (PA)



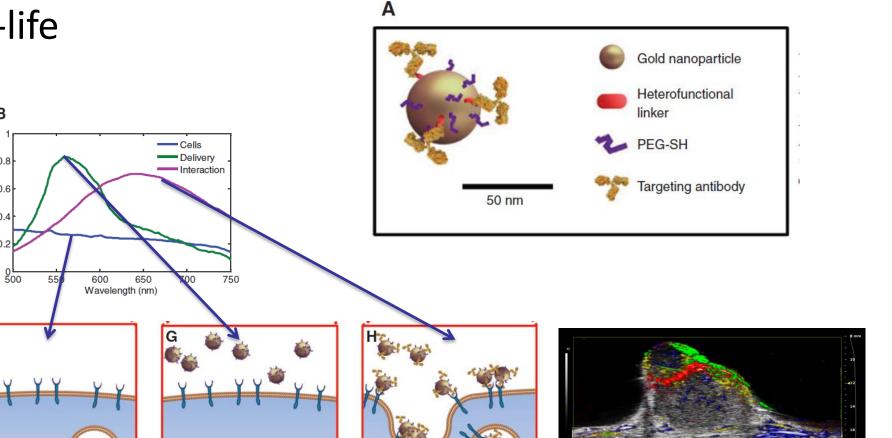
Molecular targeting Biodistribution Half-life

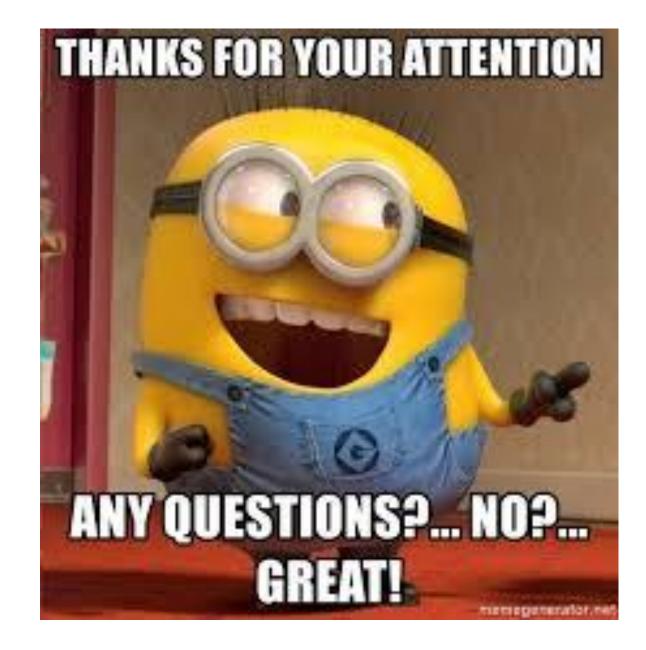
В

Scattering intensity (a.u.)

F

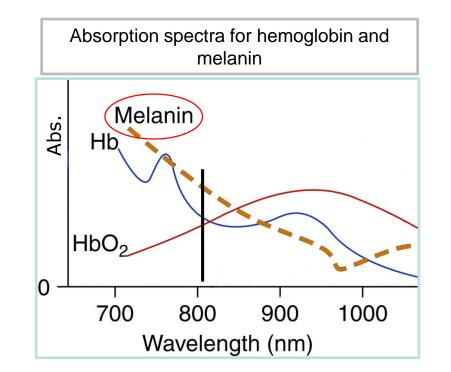
Targeted gold nanospheres



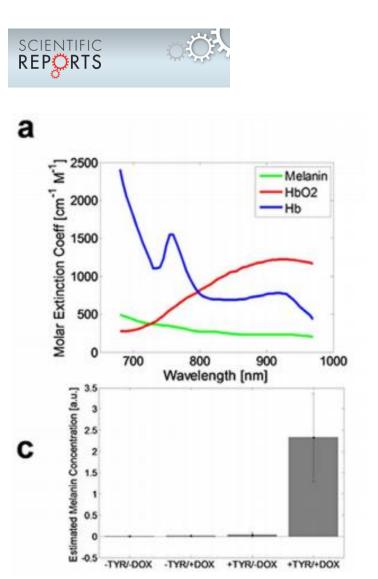


Reporter gene imaging with Photoacoustics

- **Tyrosinase**, the enzyme responsible for **melanin** production was used as an inducible reporter
- Animals with TYR- and TYR+ tumors on each flank were imaged before and after induction of tyrosinase expression







Multi-wavelength photoacoustic imaging of inducible tyrosinase reporter gene expression in xenograft tumors

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¹Department of Electrical and Computer Engineering, University of Alberta, Edmonton, Alberta T6G 2V4, Canada, ²FUJIFILM VisualSonics, Inc., Toronto, Ontario M4N 3N1, Canada, ³Department of Oncology, University of Alberta, Edmonton, Alberta T6G 122, Canada.

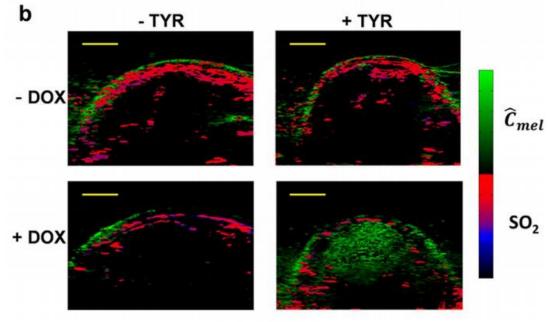


Figure 5 | Multispectral photoacoustic imaging of -TYR and +TYR tumors. (a) Molar extinction spectra of eumelanin monomers, oxy-hemoglobia (HbO₂) and deoxy-hemoglobin (Hb). (b) Multispectral photoacoustic imaging of -TYR and +TYR tumors. The green colormap represents estimated melanin concentration while the red-to-blue colormap is hemoglobin oxygen saturation. Scale bars represent 2 mm. (c) Quantitation of estimated relative melanin concentration levels using multispectral photoacoustic imaging.